



Tissue Engineering in Filtering Surgery and Future Application

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Letter to Editor

Tissue engineering involves the combination of a polymer scaffold with a population of stem, progenitor or precursor cells. Growth of the tissue in question is modeled to favor the development of a particular structure and, if the polymer scaffold used is biodegradable, it can result in the formation of structures which are remarkably similar to normal tissue (Young et al 2005). Engineered scaffolds can also be used to repair poorly-healed wounds and to fill tissue defects by their intrinsic characteristics. The application of a scaffold without cell seeding for a poorly healing wound or a large burn area can get satisfactory clinical results by enabling tissue to grow back. Connective tissue regeneration (skin, bone, cartilage) can be achieved more easily than functional tissues (liver, lung). Although most connective wounds can repair themselves, they suffer from scar formation which may lead to partial or total functional loss. Severe scar formation in some tissue is the major reason of surgical failure, an example in ophthalmology being the encapsulization of the bleb after trabeculectomy. Increasing resistance caused by scarring between the anterior chamber and subconjunctival space will slow down the effect of drainage of humors to the subconjunctival space, and result in elevated intraocular pressure. The dense and parallel deposition of secreted collagen during the natural wound healing process results in the failure of the filtering surgery. In contrast, randomized new collagen, guided by the porous structure of a subconjunctivally implanted scaffold during healing, can create a physiologic collagen deposition that can succeed in lowering the intraocular pressure [1-3].

The cellular alignment of the cornea is different from that of the conjunctiva. A parallel alignment of keratocytes and collagen in the stroma result in its transparency. In natural wound healing of the cornea, the myofibroblasts transformed from the fibroblasts migrate in the desired parallel manner, but due to their higher density, there is still no transparency [4,5]. When a randomized porous scaffold is applied in a corneal wound, this tissue engineering achieves a thicker cornea but it is still hazy due to the randomized non parallel structure.

Apart from the way the cells grow into the scaffold, the speed of degradation can also affect the healing result. In corneal wound healing both myofibroblasts and keratocytes grow from the limbus and cover the whole wound area gradually, moving from the perimeter inwards. In contrast, the scaffold might be infiltrated with inflammatory cells from the outset, causing degradation over the entire implant. By the time the myofibroblasts and keratocytes reach the center of the wound, the scaffold might already be completely degraded. It will be a big challenge for the researcher to create a stable and appropriate environment for cell migration and differentiation.

The principle of tissue engineering is to use controlled factors to produce a designed structure. By controlling all factors related to the extracellular matrix, the researcher can regulate the cellular migration and differentiation and improve the outcome of wound healing. Not only are the structure of scaffold but also the timing of degradation important to the outcome.

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